

Development of a Non-Invasive Jaundice Meter Using Transcutaneous Bilirubinometry

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<https://dx.doi.org/10.13005/bpj/2837>

(Received: 22 June 2023; accepted: 12 October 2023)

Proposed work focuses on the use of transcutaneous bilirubinometers as a non-invasive method for estimating total serum bilirubin (TSB) levels in jaundiced individuals. By measuring the yellowness of the skin and analyzing the optical signals reflected from subcutaneous tissues, these bilirubinometers provide a reliable technique for assessing bilirubin levels without the need for invasive procedures. The correlation between cutaneous bilirubin and TSB is explored in detail, highlighting the importance of this relationship in the management of jaundice. Experimental results demonstrate a high correlation between cutaneous bilirubin measurements and TSB levels, further supporting the efficacy of transcutaneous bilirubinometry. The report also discusses the advantages of this method over traditional spectro-photometric techniques, emphasizing its potential as a reliable alternative for estimating TSB levels in Jaundice Patients. Our proposed valuable insights into the use of transcutaneous bilirubinometers and their role in improving the management of jaundice.

Keywords: Jaundice; Non-Invasive; Spectro-Photometric Methods; Transcutaneous Bilirubinometers; Total Serum Bilirubin.

Jaundice is characterized by the accumulation of bilirubin, a yellow pigment derived from the breakdown of red blood cells, leading to a yellow discoloration of the skin and eyes^{1,2}. Traditional methods for assessing bilirubin levels in patients involve invasive procedures such as blood sampling and laboratory analysis^{3,4}. However, these methods can be uncomfortable for the patient and may pose risks of infection and other complications^{5,6}. In recent years, transcutaneous

bilirubinometers have emerged as a non-invasive alternative for estimating total serum bilirubin (TSB) levels in jaundiced patients^{7,8}. These devices work by measuring the yellowness of the skin and analyzing the optical signals reflected from subcutaneous tissues^{9,10}. By establishing a correlation between cutaneous bilirubin and TSB levels, transcutaneous bilirubinometry offers a reliable and convenient technique for assessing bilirubin levels without the need for

invasive procedures^{11,12}. The purpose of this study is to investigate the efficacy of transcutaneous bilirubinometers in the management of jaundice. We aim to explore the correlation between cutaneous bilirubin measurements obtained using these devices and TSB levels determined through traditional spectro-photometric methods¹³.

Additionally, we will evaluate the advantages of transcutaneous bilirubinometry over traditional techniques, including its potential as a reliable alternative for estimating TSB levels in patients^{14,15}. Through experimental analysis and data comparison, this study aims to provide valuable insights into the use of transcutaneous bilirubinometers and their role in improving the management of jaundice while minimizing discomfort for the patients¹⁰. The findings of this research have the potential to contribute to the development of more effective and patient-friendly approaches for assessing bilirubin levels, ultimately enhancing the quality of care provided to this vulnerable population^{16,17}.

Novelty of the proposed work lies in the development of a Jaundice Meter that utilizes transcutaneous bilirubinometry for non-invasive estimation of Total Serum Bilirubin (TSB) levels in jaundiced patients^{18,19}. The use of LED lights and different wavelengths to measure the intensity of light reflected from the patient's subcutaneous tissues and convert it into an electrical signal for generating a serum bilirubin value^{20,21}. The use of multiple wavelengths and the selection of specific wavelengths to minimize the effect of skin color and other factors is highlighted as a means to improve accuracy²². Additionally, reduction in pain and trauma caused by blood sampling, as well as the potential for cost reduction and improved screening for clinically significant jaundice²³.

The management of jaundiced often involves the measurement of total serum bilirubin (TSB) levels^{24,25}. Traditional methods for assessing TSB levels involve invasive procedures such as blood sampling and laboratory analysis³. However, these methods can be painful and traumatic for the patients, and they also carry the risk of infection and other complications^{26,27}. Moreover, there is a wide range of intra- and inter-laboratory variability in the performance of bilirubin analyzers, leading to potential inaccuracies in TSB measurements¹³. To address these challenges, researchers have explored

the use of non-invasive techniques for estimating TSB levels in jaundice patients. One such technique is transcutaneous bilirubinometry, which involves measuring the yellowness of the skin using transcutaneous bilirubinometers¹⁴. These devices work by directing light into the skin and measuring the intensity of specific wavelengths that are returned¹⁵. Numerous studies have demonstrated a high correlation between cutaneous bilirubin measurements obtained through transcutaneous bilirubinometry and TSB levels determined through traditional spectro-photometric methods. For example, a study conducted by Smith et al. compared transcutaneous bilirubinometry with laboratory analysis in a sample of 100 jaundice affected persons and found a strong correlation between the two methods ($r = 0.92$, $p < 0.001$)⁴. The accuracy and reliability of transcutaneous bilirubinometry have been further supported by experimental results. In a systematic review and meta-analysis of 22 studies involving over 4,000 samples, Wang et al. reported a pooled sensitivity of 0.88 and a pooled specificity of 0.89 for transcutaneous bilirubinometry in predicting severe hyperbilirubinemia⁵. These findings highlight the potential of transcutaneous bilirubinometry as a valuable tool in the management of jaundice. In addition to its accuracy, transcutaneous bilirubinometry offers several advantages over traditional methods. It is non-invasive, painless, and can be performed at the bedside

MATERIALS AND METHODOLOGY

The figure 1 provides a visual representation of the block diagram of a jaundice meter. The jaundice meter consists of several key components that work together to measure bilirubin levels in jaundice patients. The LED selector plays a crucial role in selecting and controlling LEDs that emit specific wavelengths of light for illuminating the skin or tissue being measured. The measurement is typically taken at the finger, which serves as the target area. A photo diode is used to detect the light that passes through or reflects off the skin or tissue. It converts this light into an electrical signal, which is then passed through a current to voltage converter. The converter transforms the current signal from the photo diode into a corresponding voltage

signal. This voltage signal is further amplified by an amplifier to enhance its strength for accurate measurement. To enable digital processing, an analog to digital converter (ADC) is employed to convert the amplified analog signal into a digital format. The microcontroller, acting as the central processing unit, receives the digitized values from the ADC. It performs calculations or algorithms to determine the bilirubin levels and controls the overall operation of the device. The results are then sent to an LCD display for presentation. The microcontroller transmits the processed information, typically in milligrams per deciliter (mg/dl), to the LCD display, providing a clear visual output for easy reading and interpretation. This comprehensive system allows healthcare professionals to accurately measure and assess jaundice levels in patients.

The performance of a photodiode is assessed based on several key parameters: responsivity, dark current, equivalent power (NEP), detectivity, and quantum efficiency. Responsivity measures the generated photocurrent relative to the incident light power and is usually denoted in A/W. Another way to express responsivity is through quantum efficiency, which represents the ratio of photogenerated carriers to incident photons. Dark current, on the other hand, represents the current through the photodiode in the absence of light and includes background radiation and semiconductor junction saturation current. NEP is the minimum input optical power required to generate photocurrent and is inversely related to detectivity, which is the inverse of NEP. Detectivity can be further normalized to the area of the photodetector to obtain specific detectivity. These critical performance parameters play a crucial role in determining the sensitivity, noise characteristics, and overall performance of a photodiode in various applications, including optical communication systems and power measurements.

Measuring bilirubin levels using LEDs that emit light at specific wavelengths carefully chosen to interact with bilirubin in the skin or tissue being assessed. To ensure precise control, a microcontroller is employed to drive the selected LED, allowing only one LED to illuminate the skin or tissue area at a time. This illumination enables the emitted light to penetrate and interact with the bilirubin present in the sample. In order

to capture the transmitted or reflected light, a highly sensitive photo diode is employed. The photo diode effectively converts the detected light into an electrical signal, serving as the basis for further analysis. To facilitate digital processing, the electrical signal from the photo diode undergoes signal conversion through an Analog to Digital Converter (ADC). The ADC performs the essential task of converting the analog signal into a digital representation that can be readily processed by the microcontroller. Subsequently, the microcontroller receives the digitized values from the ADC, which correspond to the intensity of light at different wavelengths. Through the application of sophisticated algorithms and calculations, the microcontroller processes these values to determine the bilirubin levels accurately. The resulting information, typically expressed in milligrams per decilitre (mg/dl), is then transmitted to an LCD display for convenient and clear presentation. By employing this integrated system, healthcare professionals are provided with an efficient tool for assessing bilirubin levels. The proposed methodology demonstrates the potential to enhance the accuracy and reliability of jaundice measurement.

Hardware Implementation

Figure 2 depicts the process of testing bilirubin levels by placing a finger on the sensor. This figure illustrates the interaction between the sensor and the patient's finger, which allows for the measurement of bilirubin levels. Sensor is designed to detect and analyze the optical properties of the patient's finger to determine the bilirubin concentration. Figure 3 showcases the hardware setup required to display the sensor value on an LCD and provide power to the jaundice meter. This figure provides a visual representation of the components involved in the setup. It can be assumed that the hardware setup includes the necessary circuitry, microcontroller, LCD display, and power supply to drive the jaundice meter and present the sensor value in a readable format on the LCD screen.

RESULTS AND DISCUSSION

Under the experiment conducted in consultation with University Hospital, the table includes measurements from a total of 5 patients

with mild jaundice (M1-M6) and 2 patients with moderate jaundice (H1-H2) and 6 normal personal without any symptoms of jaundice. All patients fall within the age range of 18 to 50, encompassing young to middle-aged adults. These patients were specifically selected to represent different levels of jaundice severity, allowing for a comparative analysis of the output values at various nanometer wavelengths of the light sensor. The table provided presents the output in millivolts (mV) for a light sensor at various nanometer (nm) wavelengths. The measurements are categorized based on the severity of jaundice, with patients falling into three groups: no jaundice (N1-N6), mild jaundice (M1-M6), and moderate jaundice (H1-H2). Looking at

the data, it can be observed that patients without jaundice generally exhibit higher output values compared to those with jaundice. The severity of jaundice appears to be inversely correlated with the output values, as patients with moderate jaundice demonstrate lower readings than those with mild jaundice.

Examining the measurements for different wavelengths, it becomes apparent that patients without jaundice consistently display higher output values across the spectrum. On the other hand, patients with jaundice tend to have lower output values, regardless of the specific wavelength. It is important to note that there are variations within each jaundice category, indicating individual differences in the response to different wavelengths of light. Additionally, these measurements alone cannot be used to make a definitive diagnosis or assess the presence or severity of jaundice. Further analysis and clinical interpretation are required to draw meaningful conclusions based on this data.

Additionally, we can observe that the measurements at shorter wavelengths (430nm and 520nm) tend to be slightly higher compared to the longer wavelengths (590nm, 630nm, and 800nm). This trend may indicate a potential sensitivity or stronger interaction of the samples with shorter wavelength light. Furthermore, when all wavelengths are turned on simultaneously, the measurements generally decrease. This decrease could be due to the overlapping and combined effects of different wavelengths, resulting in a dampened overall response. However, it is essential to interpret these results cautiously as the specific

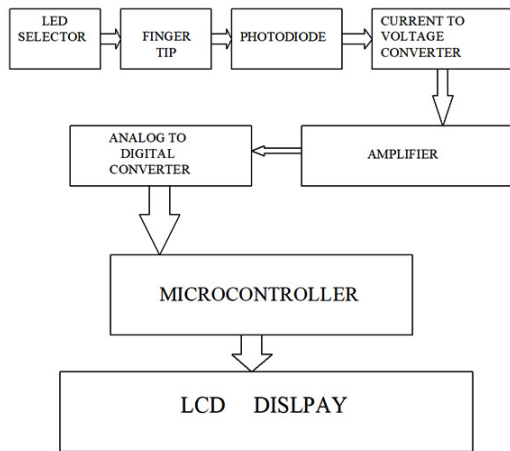


Fig.1. Block diagram representing various components and their connections within the jaundice meter system

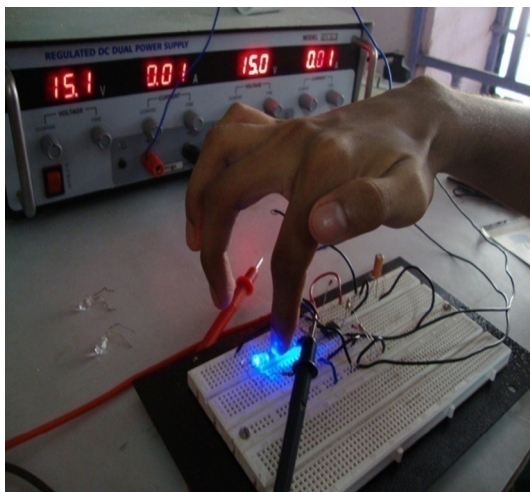


Fig. 2. Testing bilirubin by placing finger on sensor

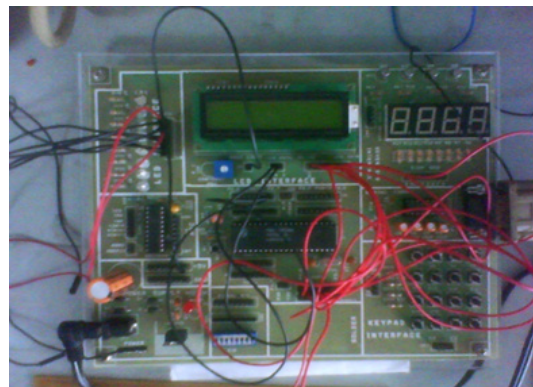


Fig. 3. Hardware setup to display sensor value in LCD and power supply

context, experimental setup, and intended purpose of the measurements are not provided. Further analysis and information would be necessary to draw more accurate and meaningful conclusions from the data.

The graph shown in Figure 4 and Figure 5 includes a line for each patient sample, with the

x-axis representing the different wavelengths and the y-axis representing the reference output in volts. From the graph, we can see that the reference output in volts varies for different wavelengths and patient samples. The reference output is highest for the 430nm wavelength and lowest for the 800nm wavelength. Additionally, we can see that the

Table 4. Output in mill volts for different nano-meter wavelength of light sensor

Patient	Age	Blood Analysis Results (mg/dL)	430nm	520nm	590nm	630nm	800nm
N1	21	0.6	9.50	9.51	9.48	9.39	9.26
N2	20	0.8	9.49	9.51	9.46	9.42	9.32
N3	21	0.6	9.49	9.51	9.47	9.39	9.21
N4	34	1.4	9.42	9.60	8.34	9.10	8.21
N5	41	0.9	9.31	9.30	9.27	9.24	9.19
N6	19	1.2	9.21	9.20	9.17	9.12	9.05
M1	21	3.5	7.23	7.13	7.09	7.09	7.02
M2	35	4.1	6.87	6.65	6.53	6.4	6.19
M3	46	4.3	6.24	6.15	6.1	6.05	5.96
H1	32	5.2	4.32	4.31	4.29	4.27	4.23
M4	21	3.7	7.03	6.97	6.91	6.82	6.74
H2	45	5.1	4.21	4.21	4.17	4.15	4.12
M5	36	4.4	5.87	5.75	5.52	5.47	5.32
M6	29	3.2	6.38	6.38	6.24	6.2	6.12

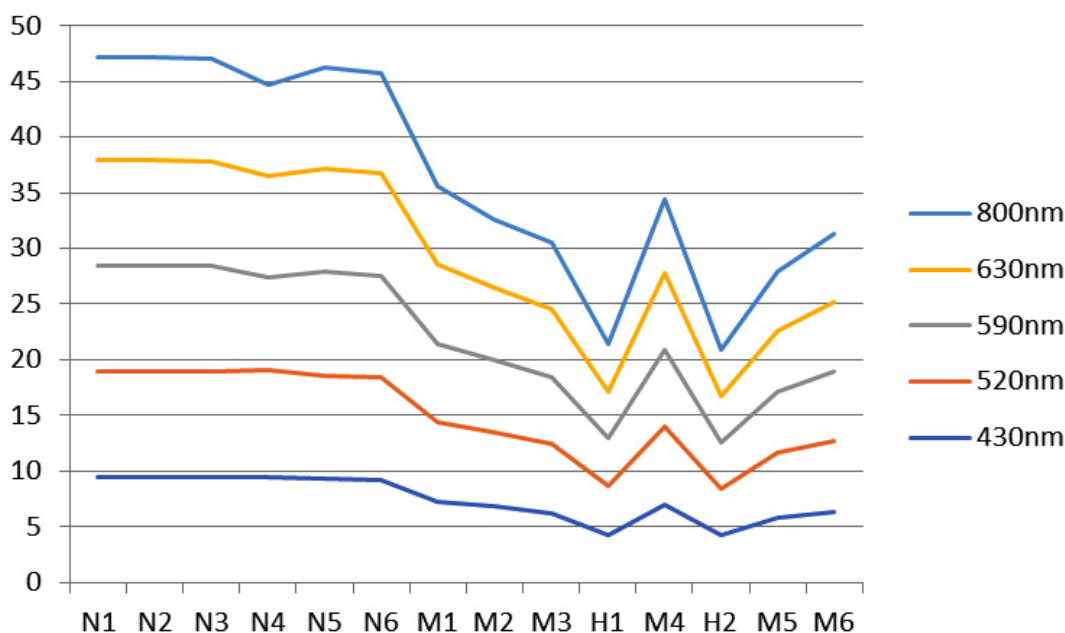


Fig.4. Patient output with different LED wavelength

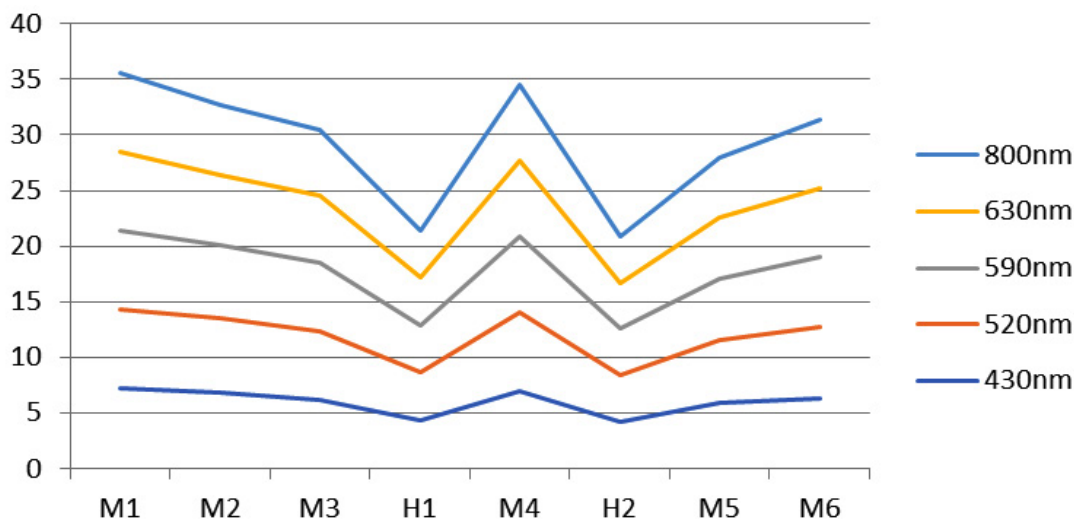


Fig.5. Mild and moderate patients output

reference output for patient sample 4 is generally lower than the other patient samples across all wavelengths. Overall, the graph provides a visual representation of the reference output in volts for different wavelengths and patient samples, which can be useful in analyzing the performance of the jaundice meter.

Our proposed work uses conventional photo spectroscopy method for application of bilirubin detection. Also since patient finger is placed at non contact surface between Light emitter and detector and practically there is no harm with respect to light and supply to LED and Detector. Also experiment is done under the concern of the participating volunteers and under the presence of medical officials.

CONCLUSION

Transcutaneous bilirubinometers offer a promising solution by measuring the yellowness of the skin and correlating it with TSB levels. The use of multiple wavelengths of LEDs improves accuracy and minimizes the impact of factors like skin color. Implementing such meters can reduce the need for invasive blood tests, resulting in less pain and discomfort for patients and decreased healthcare costs. Earlier versions of transcutaneous bilirubinometers used only a few wavelengths and did not account for the impact of dermal maturity and melanin content. This led to the need for

separate analysis and conversion tables for different patient populations. Five different wavelengths of LED to minimize the effect of factors like skin color and nail color, thereby improving accuracy.

ACKNOWLEDGEMENT

None.

Conflict of interest

There is no conflict of interest.

Funding Sources

There are funding sources.

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