Multi Modalities Medical Image Fusion Using Deep Learning and Metaverse Technology: Healthcare 4.0 A Futuristic Approach

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Multimodal medical image fusion is the efficient integration of various imaging modalities to improve the ability to assess, direct therapy, treat patients, or predict outcomes. As image fusion offers additional essential information, the correctness of the image generated from different medical imaging modalities has a substantial impact on the success of a disease's diagnosis. A single medical imaging modality cannot provide complete and precise information. In the modern research area, multimodality medical image fusion approach is one of the meaningful research in the area of medical imaging and radiation medicine. The fusion of medical images is the process of enrolling and combining multiple images from one or more imaging modalities, enhancing the image quality and to achieve randomness and redundancy, heighten the clinical utility of medical images in the diagnosis and evaluation of medical problems. The thought is to enhance the image occurrence Magnetic resonance imaging (MRI) is achieved by combining images like computerized tomography (CT) as well as magnetic resonance imaging (MRI) gives fine soft tissue information as long as CT gives fine facts over denser tissue. In this research paper, we have an account that features for future development with demanding performance requirements and processing speed.

**Keywords:** Discrete Wavelet Transform, Image Fusion, Multimodality, Quality Measurement Technique, Spatial Domain, Transform Domain.

Uncommonly, images have independent or defined content of information. Images of various sorts reflect various forms of information. It produces the information that is dispersed and impairs the doctor’s judgment. This issue has drawn the interest of an abundance of experts in the area of medical diagnosis. Image fusion is an efficient technique which can be done automatically determine the data contained in unlike images as well as incorporate them to yield
one composite image containing all of the objects at stake that are simple and clear. Yet, the overall performance of diagnosis is determined by the visual quality but also by information contained in medical images. Presently, there are various imaging modalities attainable to acquire particular medical information of a specific organ by human brain X-ray, positron emission tomography, MRI, and CT, as well as computed tomography based on single-photon emission (SPECT) images revealed in Figure 1 are vital medical imaging techniques through them. The image fusion mechanism is capable of efficiently taking action on this challenge. Enriching the data provided by merging the additional information given by combining two may be more modalities to create a single image.

The medical images collected from sensors from various sources are fused in order to enlarge the diagnostic image modality’s quality. From 2016 to 2021, the technology of medical image fusion has advanced significantly, as can be seen in Figure 2.

The goal of this study is just to outline the advancement of exploration and the future advancements of this entire field, bringing it together with regard to scientific publications around fusion of medical images in modern years. This article is divided into sections listed below:

1) An overview of contemporary fusion methods
2) Discrete Wavelet Transform using Haar
3) The Proposed Fusion Method
4) Quality Measurement Technique to test the MSE, PSNR, and SSIM methods to determine their compatibility.

Fusion Methods

Depending on the spatial domain, this same fusion procedure is based on the transform domain and the deep learning fusion method.

Spatial Domain

Spatial Domain Fusion technology is being developed is not difficult, because the fusion methods can be done directly enforced to the pixels of the original image, forcing the combined image. We directly accord with pixels and cast the pixels to obtain a fused resultant image. During pixel techniques, image fusion techniques frequently guide to the nonexistence of spectral information and propose spatial alterations. It consists of many methods, such as the Mean Method and the Select Maximum Procedure, Choose the Minimalist Approach, Intensity Hue Saturation Fusion Method, etc. These methods of fusion occurs directly enforced in relation here to input images and that will reduce the final fused image’s signal-to-noise ratio by the straight forward averaging method.

Average Method

The Average method is a fusion approach used to join images by averaging the pixels. This approach is intent on all parts of the image and if the images are captured same from the same form of sensor then it works correctly. Assuming that the images have high brightness and high contrast, then it will give a good outcome.

It’s described as:

\[ F(x, y) = \frac{P(x, y) + Q(x, y)}{2} \]  

Where, \( F(x, y) \) is the final fused image, \( P(x, y) \) and \( Q(x, y) \) are two input images

Select Maximum Method

In it, the result of the fused image is attained by choosing the maximum corresponding pixel intensity in contrast to the pair of input images.

\[ F(i, j) = \sum_{M} \sum_{N} \max A(i, j) B(i, j) \]  

In this case, \( A \) and \( B \) were also input images, and \( F \) is the fused image.

Select Minimum Method

In it, the result of the fused image is attained by choosing the minimum corresponding pixel intensity in contrast to the pair of input images.

\[ F(i, j) = \sum_{M} \sum_{N} \min A(i, j) B(i, j) \]  

In this case, \( A \) and \( B \) were also input images, and \( F \) is the fused image.

Intensity Hue Saturation (HIS) Fusion Method

The three attributes of a specific color that create a regulated visual representation of an image are intensity, hue, and saturation. The oldest technique of image fusing is the HIS transform. Hue and Saturation contain most of the spectral information and must be carefully controlled in HIS space. It has certain characteristics: (1) the intensity additive has nothing to do with the
image's information on color. (2) Saturation and hue additives are carefully associated with the manner human beings understand color\textsuperscript{13}. Hence, this technique is used to figure out the color issue in the image fusion steps.

Transform Domain

Transformation Domain Medical image fusion method is primarily according to the theory of multi-scale transformation (MST). The transformation domain-based method of fusing medical images translates original image taken from the time domain to obtain a low frequency domain or any other domains and high-frequency coefficients\textsuperscript{14}.

The most frequently used transform domain fusion techniques for medical images:
- Discrete Fourier Transform
- Discrete Cosine Transform
- Discrete Wavelet Transform

Discrete Fourier Transform

It is crucial that image processing software is used to break down an image transformed into cosine and sine elements. The result of the transform represents a Fourier transform as well as a frequency range image, but the input image is the same as an image in real space. In the image of the Fourier domain, a particular point shows a specific frequency composed of the image of the spatial domain. It is utilized in broad applications such as image reconstruction, image filtering, and image compression are all examples of processing images\textsuperscript{15}. In the case of an oblong representation of size $N \times N$, in two dimensions, DFT is described as:

$$F(k, l) = \sum_{i=0}^{N-1} \sum_{j=0}^{N-1} f(i, j) e^{-2\pi \frac{(ki + lj)}{N}}$$ \hspace{1cm} \text{(4)}$$

This can be an equation explained as the worth of points $F(k, l)$ is captured, such as adding to a spatial picture appropriate primary performance and adding the results.

The basic objective with cosine and sine waves rising frequencies, i.e. $F(0,0)$ means the image’s DC element correlates in comparison to the typical brightness, as well as $F(N-1, N-1)$ reflects the frequency at its peak.

At the same, the Fourier representation could be changed back into the area of space. Fourier’s inverse convert is defined as:

$$f(a, b) = \frac{1}{N^2} \sum_{k=0}^{N-1} \sum_{l=0}^{N-1} F(k, l) e^{2\pi \frac{(ka + lb)}{N}}$$ \hspace{1cm} \text{(5)}$$

Take note of $1/N^2$. The reverse conversion includes a normalization term. To achieve a result from the above equation, a double sum must be calculated from a particular point of view. However, because the Fourier Transform seems to be separable, it could be used separately and described as:

$$F(k, l) = \frac{1}{N} \sum_{b=0}^{N-1} P(k, b) e^{2\pi \frac{lb}{N}}$$ \hspace{1cm} \text{(6)}$$

As,

$$P(k, b) = \frac{1}{N} \sum_{a=0}^{N-1} f(a, b) e^{2\pi \frac{ka}{N}}$$ \hspace{1cm} \text{(7)}$$

Applying both of these equations, an image in the spatial domain is represented first by converting and using N Fourier transforms in one dimension, create an image in the middle. After that, the middle image is converted from the finished image, repeatedly adopting there are N Fourier Transform in one dimension. Compelling the 2-D regarding a Fourier Transform sequence of 2N 1-dimensional transforms reduces the quantity of needed approximation\textsuperscript{16}.

Transforming Fourier outcomes is an output image with a complex numerical value that can be shown because of two images, either genuine or made up of parts or size and polarity. Only the size of an image processing employs the Fourier Transform process, usually as it is displayed, consists of the majority of the data on the geometrical design of the image in the spatial domain.

Discrete Cosine Transform

DCT is a 4-step transformation coding method. The source image is first divided into sub-blocks measuring 8 * 8 pixels\textsuperscript{17}. Then, each block is converted to a frequency domain representation using a 2-dimensional DCT basis function. The
following frequency coefficients are quantized and lastly, lossless entropy encoder output. DCT is an efficient image compression method because it can de-correlate image pixels.

The equation for 1-DCT
\[ x_k = \frac{1}{\sqrt{N}} \left( x_0 + \sum_{n=1}^{N-1} x_n \cos \left( \frac{\pi}{N-1} n k \right) \right) \]

Where, \( k = 0,1 \ldots N-1 \)

The equation for 2-DCT:
\[ X_k = \sum_{n=0}^{N-1} x_n \cos \left( \frac{\pi}{N} (n+\frac{1}{2})k \right) \]

Here is Figure 4, which provides the basic idea of DCT.

**Discrete Wavelet Transform**

It is a time domain analysis approach with a fixed window size and convertible forms. In the high frequency section of discrete wavelet transform converted signals, the time differentiated rate is excellent. In addition, the frequency differentiation rate in the low frequency section is good. It is capable of successfully extracting information from a signal.

Figure 5 depicts a two-channel, one-dimensional filter bank for perfect reconstruction. Filters for low and high analysis are utilized to convolve the input discrete sequence \( x \). Each of the two down sampled signals, \( x_H \) and \( s_L \) is transformed according to the algorithm. For well-created filters, \( x \) is a signal precisely reconstructed \( y=x \).

In a 2-Dimensional Discrete Wavelet Transform, a 1-Dimensional DWT is performed in rows first, then by using filters but also down sampling data columns separately. These outcomes are in three types of detail coefficients and one specify of approximation coefficient describing the diagonal, vertical, and horizontal, planes of the image. To theory of filter terminology, four of these secondary images are equivalent toward the results of the low-low (LL), low-high (LH), high-low (HL), high-high (HH) bands. Fig.6 represents an image decomposition on a single level \( f(x, y) \) into four sub-bands LL, LH, HL, HH. Hence, a DWT with \( N \)-levels of degradation will have \( M = 30N + 1 \) similar spectrum bands. Figure 6 shows the 2-Dimensional Wavelet Transform structures with a single level of decomposition.

The statement for the 2-D DWT in the image is given by
\[ \frac{1}{\sqrt{a}} \sum \sum f(x, y) \Psi \left( \frac{x-m}{a}, \frac{y-n}{b} \right) \text{d}x \text{d}y \]

Where \( m \) and \( n \) parameters relocate and \( a \) is a scaling factor \( \Psi(m,n) \) transform using the Haar wavelet.

Figure 7 represents the components using a two-channel two-filter bank for perfect dimensional reconstruction.

**DWT Using Haar**

This is the merged image with multiple scales for each level of the image, merging the correlations to get a highest, lowest, or average blending path for every image. The concluding next would be the image reconstruction of images to obtain the concluding merged image by applying

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**Fig. 1.** Classification of different multi-model imaging.
IDWT to the output value multiplied by the level of obtaining the output as depicted in figure8.

**Deep Learning**

In recent years, the study of image fusion has expanded to include deep learning. One popular deep learning model is the convolutional neural network. The activity level measurement (feature extraction) and fusion rules deficiencies in spatial and transform domain-based image fusion approaches necessitate artificial design, and the association between them is negligibly minor. Convolutional neural network is a trainable supervised learning multistage feed forward artificial neural network. Convolution is a multidimensional operation. In a convolutional network, the primary parameter is typically known as an input, and the second parameter is known as a kernel function, and the output is known as a function map. Sparse representations, parameter sharing, and isomorphic representations are the three main architectural ideas of convolutional neural networks.

However, convolutional networks and types of sparse representation of neurons connect only to a few neighboring neurons.
in the previous stage and perform local convolution operations, thus reducing memory requirements and increasing computational efficiency. The CNN stage has constant weights and better memory requirements than other stages.

**Convolutional Neural Network**

Since medical images have different intensities at the same points, the fusion approach proposed isn’t always appropriate for scientific picture fusion. This approach makes use of the Siamese network to create a weight map. Since the two weight branches are the same, the function extraction or pastime stage size strategies of the supply image are the same. It has advantages over pseudo-Siamese and two-channel models, and the ease of training Siamese models is also the reason why they are preferred for fusion applications. After getting the weight maps, Gaussian pyramid rework is used and pyramid transform is used for multi-scale decomposition, so the merging process is more consistent with human visual perception. Furthermore, we adaptively adjust the decay coefficients using a localized similarity-based fusion strategy. This combines the pyramid

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**Fig. 4. Basic idea of DCT**

**Fig. 5. A two-channel perfect reconstruction filter bank**

**Fig. 6. 2-D DWT multi-resolution images decomposition**
and similarity-based fusion algorithms with the CNN model to produce a superior fusion method. Figure 9 is an example algorithm.

**Metaverse**

“Metaverse” is a term that refers to the digital world that exists outside the real world. It can be viewed as a 3D virtual world that allows users to interact and engage with each other. It is based on blockchain technology and uses crypto currencies known as exchange traded commodities (ETPs) to pay for goods and services. The metaverse is still in active development. A three-tier architecture is shown in fig. 10. A fundamental requirement of the metaverse is that the architecture must move from the physical world to the virtual one.

Some of the key promises of the metaverse are:

- Decentralized world: Metaverse is a decentralized world where users can manage their own data.
- Identity verification: Metaverse uses blockchain technology to verify user identities and ensure that only authorized users can access data.
- Smart contracts: The metaverse uses smart contracts to automate transactions.
- ETPs: Metaverse native crypto currencies can be used to pay for goods and services, or reward AI applications for task completion.

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**Fig. 7.** DWT structure with labeled sub bands

**Fig. 8.** Fusion process of DWT using Haar

**Fig. 9.** Schematic diagram based on CNN fusion algorithm
Table 1. Results of all different fusion techniques

<table>
<thead>
<tr>
<th>No.</th>
<th>Fusion Techniques</th>
<th>MSE</th>
<th>PSNR</th>
<th>SSIM</th>
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<tr>
<td>1</td>
<td>Mean, Mean</td>
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<td>1.223</td>
<td>1.10</td>
</tr>
<tr>
<td>2</td>
<td>Mean, Max</td>
<td>0.2134</td>
<td>2.333</td>
<td>2.20</td>
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<tr>
<td>3</td>
<td>Mean, Min</td>
<td>0.3332</td>
<td>1.273</td>
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<tr>
<td>4</td>
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<td>0.2232</td>
<td>2.423</td>
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<td>9</td>
<td>Min, Mean</td>
<td>1.3232</td>
<td>3.223</td>
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</tr>
</tbody>
</table>

Fig. 10. Three-layer Architecture of the Metaverse

Fig. 11. The flowchart steps for the proposed image fusion
The Proposed Model

The suggested approach is a multimodal utilized fusion specifically for images in medicine. This method seeks to achieve more clinically relevant use of medical imaging for the evaluation and evaluation of health issues by reducing redundant work, and improving quality.

An issue needs to be resolved first by starting images with how to process and obtain the best image match from the suggested method. This is because the images that were taken by the patient are divided into various shapes and sizes. Choosing and finding the ideal match between images is really challenging for the naked eye, so prior to applying any proposed technique, we need to order that match. The subsequent algorithm flowchart is presented as shown in figure 11.

Flow chart for the Proposed Image Fusion Method

The process starts by analyzing the image utilizing data from two different sources finding various sizes. If the operation does not connect, the action stops, but if the size matches, the activity continues. Then, by identifying the difference in error between each tested image, the variation between the two images is determined, and the best following match between the two images is determined. They apply DWT as a future step to splitting the two images into four coefficients at a predetermined level and approach every level coefficient. Applying yields the final fused images, the Inverse Discrete Wavelet Transform (IDWT) as an interpretation of the fusion of the image.

Proposed Image Fusion Algorithm

The suggested procedure a definition of an algorithm in stages like this:

Step 1: Read the images from CT and find the size.
Step 2: Read the images from the MRI and find the size.
Step 3: Find the best matching images.
Step 4: Apply discrete wavelet transform.
Step 5: Apply the fusion selection rule to the images.
Step 6: Take the inverse discrete wavelet transform.
Step 7: Get a fused image of the output.

Quality Measurement Technique

In this research paper, we have to test the MSE, PSNR and SSIM methods to determine their compatibility. There are various ways to improve image quality widely used to access peak signal over noise ratio, universal image quality index, and mean square error, among others, Human Vision System, Features Similarity Index Technique, Structured Similarity Index Technique etc.

Mean Square Error (MSE)

It represents the squared mean difference between the original image and the filtered image. The roots you can estimate mean square error in one of several methods to measure the disparity between the values of an estimate as well as the actual certificated quality. Mean Square Error is provided by the following formula, in which M and N are dimensions (width and height) of the images, the improved image I (i, j), as well as the original image K (i, j). The row or column pixel of the basic and improved image is represented by the letters i and j.

\[ \text{MSE} = \frac{1}{M \times N} \sum_{i=0}^{M-1} \sum_{j=0}^{N-1} (I(i, j) - K(i, j))^2 \]

If the MSE detects two identical images, it is zero. The PSNR for this value is not defined (zero division). An image the same as the original produces an unclear PSNR, given that the MSE becomes zero due to a division-by-zero error.

Peak Signal-To-Noise Ratio (PSNR)

The maximum signal-to-noise ratio is the ratio peak power of an indication of the loudness the signal’s strength. In order to gauge how well the motion estimation method performs in the suggested system, PSNR. As a metric, the peak based on the mean square error has been employed of quality and the following calculation can be used to determine its value:

\[ \text{PSNR} = 10 \log_{10} \left( \frac{\text{peakval}}{\text{MSE}} \right) \]

Structure Similarity Index Measure (SSIM)

SSIM is used to determine the degree of resemblance between two images. It is the measurement of image quality using an original
reference or noise-free image as a baseline and a noisy image as a deformed image. In this, two images are compared based on luminous, contrast and structure\cite{14}. The equation that is used to calculate the value of two images A and B is:

\[
SSIM(x, y) = \frac{(2\mu_A\mu_B + C_1)(2\sigma_{AB} + C_2)}{\mu_A^2 + \mu_B^2 + C_1}(\sigma_{A} + \sigma_{B} + C_2)
\]

\text{(14)}

Where, \( \mu_A \) and \( \mu_B \) are the functions of \( x, y \), \( \sigma_A^2 \) and \( \sigma_B^2 \) are the variances, \( \sigma_{AB} \) is the covariance.

**RESULTS**

Images include the presence of axial brain tumor (MRI) and CT. After receiving the fused image, we have to test the MSE, PSNR and SSIM. The results are described in Table 1.

**CONCLUSION**

In image processing, IQA is crucial. There are several sorts of image quality metrics in use for determining image quality. The optimum quality metric is obtained in this article by using MSE, PSNR, and SSIM. This paper combines images using a DWT and the average rule. The fused image quality is improved by testing and analyzing by using metrics. Different medical services, including illness prevention, healthcare, disease diagnosis and treatment, management of chronic diseases, consultation, etc., could be facilitated by the interaction between virtual and real cloud professionals and terminal users.

**Conflict of Interest**

There is no conflict of interest.

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**REFERENCES**


