Estimation of Number of Levels of Scaling the Principal Components in Denoising EEG Signals

B. Krishna Kumar

Department of ECE, Methodist College of Engineering and Technology, Hyderabad-500001, Telangana State, India. *Corresponding author E-mail: saisantu2004@yahoo.co.in

https://dx.doi.org/10.13005/bpj/2142

(Received: 01 June 2020; accepted: 16 January 2021)

Electroencephalogram (EEG) is basically a standard method for investigating the brain's electrical action in diverse psychological and pathological states. Investigation of Electroencephalogram (EEG) signal is a tough task due to the occurrence of different artifacts such as Ocular Artifacts (OA) and Electromyogram. By and large EEG signals falls in the range of DC to 60 Hz and amplitude of $1-5 \mu v$. Ocular artifacts do have the similar statistical properties of EEG signals, often interfere with EEG signal, thereby making the analysis of EEG signals more complex[1]. In this research paper, Principal Component Analysis is employed in denoising the EEG signals. This paper explains up to what level the scaling of principal components have to be done. This paper explains the number of levels of scaling the principal components to get the high quality EEG signal. The work has been carried out on different data sets and later estimated the SNR.

Keywords: Principal components, PCA, Multi scale PCA (MSPCA), Denoising, and SNR.

The study of Electroencephalogram is very much helpful in diagnosing different disorders of the nervous system. EEG is the electrical action recorded from the scalp surface, which is picked up by conductive media and electrodes1-3. EEG has been performing a vital role in investigating brain activities in clinical application and scientific research for several years⁴⁻⁶. The EEG signals can be contaminated by various artifacts, of which the major noise source is ocular artifact, which includes Eye-movement and eye-blink's7. However, artifacts are the major enemies of high-class EEG signals. The mixing up of these ocular artifacts with the EEG signal at the time of recording causes the problems in the accurate estimation of EEG signal. These artifacts will plunge into either of the 2

categories namely, technical and physiological artifacts. Power line noise 50/60Hz falls into technical artifact category while the artifacts that crop up because of ocular(EOG), heart(ECG) and muscular activity(EMG) falls into physiological artifacts category respectively⁸.

Regression in the time domain and frequency domain⁹⁻¹¹ methods were proposed in removing eye blinks artifacts. These methods require a reliable reference channel. This channel can be contaminated by EEG. So, EEG has to be removed from the reference channel by regression techniques. Hence, the regression methods are not the finest to remove EOG artifacts.

Principal Component Analysis is one of the available techniques for extracting the information

This is an d Open Access article licensed under a Creative Commons license: Attribution 4.0 International (CC-BY). Published by Oriental Scientific Publishing Company © 2021



from the data and has found applications in a wide range of disciplines¹². PCA was introduced by Pearson in 1901¹³ and developed by Hotelling ¹⁴ in the year 1933.

In this research paper, up to how many levels the principal components have to be scaled for obtaining the better denoised EEG signal is elaborated using MSPCA and WAVELETS¹⁵ and later estimated the SNR.

METHODOLOGY

Principal component analysis

Principal Component Analysis (PCA) can be applied to EEG data that contains a large number of measured variables to develop into a smaller number of artificial variables called principal components(PC). Obtaining a smaller number of variables from a large number of measured variables is to reduce the redundancy in the measured variables. Here, redundancy means some of the variables in the measured data are correlated with one another, because they are measuring the same construct. The main idea of PCA is to reduce the dimensionality of the data set, as the data set consists of a large number of interrelated variables, and trying to retain as much as possible variation present in the data set. These principal components are uncorrelated, orthogonal and ordered in such a way that the first few components retain most variation present in all of the original variables. PCA is performed by eigen value decomposition of data covariance matrix. This is usually done after mean centering the data for each attribute.

If the variables in a data set are already uncorrelated, PCA is of no value. In addition to being uncorrelated, the principal components are orthogonal and are ordered in terms of the variability they represent. That is, the first principal component represents, for a single dimension (i.e., variable), the greatest amount of variability in the original data set. Each succeeding orthogonal component accounts for as much of the remaining variability as possible.

In other words, Principal component analysis (PCA) is a multivariate data analysis procedure that transforms a set of 'n' correlated variables, $X = (x_1, x_2...x_n)$, into a set of uncorrelated variables called principal components $(p_1, p_2, ..., p_n)$. The first principal component accounts for most of the variability in the data, while each of the succeeding components in turn account for the highest amount of the remaining variability. Each principal component is a linear combination of the

 Table 1. Principal Components at Each Level of Decomposition

 and Corresponding Principal Component Variances Vectors-[FIRST

 SCALE PCA]

Level No	Principal Components Vector At Each Level (Eigen Vectors)		PC Variances (Eigen Values)	
1	-0.71426	0.69987	0.18818	
	0.69987	0.71426	0.14141	
2	0.31328	0.94965	0.23541	
	0.94965	- 0.31328	0.17906	
3	-0.03374	0.99943	0.79591	
	-1.0332	0.55813		
4	0.33820	-0.94107	4.19395	
	0.94107	0.33820	1.61476	
5	-0.46860	0.88341	8.69436	
	-1.352	6.47539		
6	0.04964	-0.99877	11.3113	
	0.99877	0.04964	2.59938	
7	0.93849	-0.34529	136.827	
	0.34529	0.93849	11.8306	
8	-0.32884	0	1.12188	
	-0.94439	0	0.21859	

variables, X. The ith principal component can thus be expressed as

$$Var(Y_i) = e_i^T R \qquad \dots (2)$$

 $y_i = e_i^T X$...(1) where,

e, is the eigenvector of the covariance matrix (R) of X (e_i^T is the transpose of e_i).

The variance of the ith principal component is given by

$$\operatorname{Var}(Y_i) = e_i^{-1} R$$

where

 $e = \lambda_i;$ i = 1, 2...n λ_i is the ith eigenvalue.

PCA makes one stringent but powerful assumption, linearity. This assumption simplifies the problem by restricting the number of variables from the measured data. Hence PCA is used to reexpress the data, which is a linear combination of



Fig. 1(a). Original and Artifact Removed EEG Signal of Data Set 1 using First Scale PCA

427

original basis and which is explained here in terms of linear algebra.

Consider an original data set X, which is an mxn matrix, where 'm' corresponds to the number of measurement types and 'n' is the number of samples. The main goal is to find an orthonormal matrix 'P' in Y=PX such that $C_y=1/n(YY^T)$ is a diagonal matrix. The matrix 'P' transforms 'X' into 'Y'. The rows of orthonormal matrix 'P' represent principal components of original data set 'X'. **First level PCA**

Two data sets, namely, EEG data set1(X1)



Fig. 1(b). Original and Artifact Removed EEG Signal of Data Set 2 using First Scale PCA

428



Fig. 2(a). Original and Artifact Removed EEG Signal of data set1 with MSPCA

Table 2. Principal Components and Principal Component
Variances Vectors Obtained After Second Scale PCA and Wavelet
Denoising

Level No	Principal Components Vector At Each Level (Eigen Vector)		PC Variances (Eigen value)		
1	-1.4117		0.17755		
	-0.66378	0.74792	0.14424		
2	-1.353	0.18846			
	0.88226	-0.47075	0.17321		
3	-1.0353	0.73933			
	0.99936	-0.03589	0.43569		
4	0.45131	0.89237	4.01686		
	0.89237	-0.45131	1.39216		
5	0.78691	0.61707	9.15681		
	0.61707	-0.78691	5.4969		
6	0.04293	-0.99907	11.2858		
	0.99907	0.04293	2.15695		
7	0.93978	0.34178	175.298		
	0.34178	-0.93978	6.19914		
8	0.58069	0	1.27604		
	0.81412	0	0.28103		

and EEG data set2(X2), each of size 1x1000, were collected from physionet.org website¹⁶. These two data sets were down sampled by a factor of 2. This reduces the size of each data set to 1x500. Each data set is normalized using the following formula:

X=(X-mean(X))/std(X)

where, mean(X) is mean of X

std(X) is standard deviation of X

The mean of each data set is calculated using the following formula:

$$\overline{X} = \frac{\sum_{i=1}^{n} X_i}{n}$$

Where, n corresponds to number of samples in the data set X.

The variance of each data set is calculated using the following formula:

$$\sigma^{2} = \frac{\sum_{i=1}^{n} (X_{i} - \overline{X})^{2}}{n-1}$$

After obtaining the normalized data sets, a noise signal (EOG signal collected from physionet. org website), whose variance is of 0.4 and of length 500, is added to the two data sets. This results in two noisy data sets. These two noisy data sets are of size 1x500 are converted into a column vector.

The size of the column vector will be equal to 500x2. This column vector is treated as noisy EEG signal. For each column of data matrix wavelet decomposition is done to a level of 6 using



Fig. 2 (b). Original and Artifact Removed EEG Signal of data set2 with MSPCA

sym8 wavelet. The wavelet decomposition gives approximate and detailed coefficients of noisy EEG signal. At each level of wavelet decomposition, i.e., on approximations and as well as details in wavelet domain, corresponding covariance matrices are computed. For each covariance matrix, PCA is performed. After performing the PCA on each covariance matrix, at each level, the most significant Principal Components (PC'S) are selected. Here the selection of Principal Components is done using the Kaiser's rule. This rule retains the Principal Components that are associated with the Eigen values greater the mean of all Eigen values¹⁷.

The Principal Components at each level of decomposition and corresponding Principal Component variances vectors are provided in the Table 1

Principal Components (1.12188 and 0.21859) corresponding to level 8 are the number of retained principal components for final PCA after wavelet reconstruction.

From level 8, it is observed that the original data in two dimensional spaces is reduced to one dimension and shown below for ready reference.

LEVEL 8 -0.32884 0 ★ -0.94439 ★ 0 First score PC Second PC score

Using these principal components one can reconstruct the denoised version of the input matrix X. The denoised versions of the input matrix X i.e., EEG data set1 and EEG data set2 are shown in the Fig. 1 (a) and Fig. 1(b) respectively.

The quality of column reconstructions is estimated by the relative mean square error are 22.1904933458124% and 73.9497428008459%, not closer to 100%.

Since the quality of column reconstructions after first level PCA are not closer to 100%, hence the level of scaling principal components is taken to next level¹⁸. Hence retaining of principal components will be decided based on the quality of reconstruction of columns which is measured by relative mean square error.

Second level PCA

The simplified input matrix X, which was obtained from the first scale of PCA, is again decomposed to a level of 6 using sym8 wavelet. Now the wavelet coefficients obtained after the wavelet decomposition are thresholded using Heursure thresholding. For these wavelet coefficients PCA is performed and selected the significant principal components. Using these principal components one can reconstruct the much more denoised input matrix X. The quality of reconstruction of the columns estimated after the second time processing of the input matrix x are close to 100% and are 99.9981% and 99.9991%.

The principal components and Principal Component variances vectors of the two data sets obtained after second scale PCA and wavelet denoising are shown in the Table.2.

Principal Components (1.27604 and 0.28103) corresponding to level 8 are the number

Table 3. (Comparison	of SNR (of Denoised	l EEG Signal	Obtained using	MSPCA	and Different	Wavelets
				0				

Wavelet family/Threshold type	SNR (dB)
Sym8 (soft)	34.95
Sym8 (hard)	24.52
Haar (soft)	20.29
Haar (hard)	25.10
dB10 (soft)	28.89
dB10 (hard)	23.74
MSPCA (for DATA SETS-1 AND 2)	37.43
MSPCA(for DATA SETS-2 AND 3)	35.36
MSPCA(for DATA SETS -4 AND 5)	35.16
	Wavelet family/Threshold type Sym8 (soft) Sym8 (hard) Haar (soft) Haar (hard) dB10 (soft) dB10 (hard) MSPCA (for DATA SETS-1 AND 2) MSPCA(for DATA SETS-2 AND 3) MSPCA(for DATA SETS -4 AND 5)

of retained principal components for final PCA after wavelet reconstruction.

From level 8, it is observed that the original data in two dimensional spaces is reduced to one dimension and shown below for ready reference.

LEVEL 8

0.58069	0
0.81412	0 🔨
First PC score	Second PC score
~	

On comparing Table.1 and Table2 the final PC's in the level 8 are improved after second time PCA using wavelet denoising¹⁹. Using the selected principal components one can reconstruct noise free EEG signals back. The waveforms of Denoised EEG signal constructed after second scale PCA are shown in Fig 2(a) and 2(b).

RESULTS

The results obtained after performing MSPCA on different data sets were tabulated in Table 3 and also compared with the previous results¹⁸.

CONCLUSION

The MSPCA is providing better SNR as the Relative Mean Square Error(RMSE) of the columns is closure to 100%. Hence, it is important to check the Relative Mean Square Error (RMSE) of the columns before reconstructing the Denoised EEG signal and estimating the SNR.

ACKNOWLEDGEMENT

Not applicable

Conflict of Interest

There is no conflict of interest.

Funding Source

Not applicable.

Ethics Approval

This data were downloaded from Physionet data base which is an open source data base and duly acknowledged in the text.

REFERENCES

1. B. Krishna Kumar "Denoising of EEG Signals using Wavelets and SIMULINK Techniques "International Journal of Recent Technology and Engineering (IJRTE), 8(5): pp.335-339 (2020).

- 2. E. Niedermeyer and FH Silva. "Electroencephalography: Basic principles, clinical applications and related fields", Lippincott, Williams & Wilkins, (2004),
- 3. MR Arab, AA Suratgar, VMM Hernandez, AR Ashtiani "Electroencephalogram Signals Processing for the Diagnosis of Petit mal and Grand mal Epilepsies Using an Artficial Neural Network. *Journal of Applied Research and Technology*, **8**: pp. 120-129 (2010).
- GL Holmes, ad CT Lombroso. "Prognostic value of background patterns in the neonatal EEG". J. Clin. Neurophysiol, 10: pp. 323-352 (1993).
- S Almubarak, and PK Wong."Long-Term Clinical Outcome of Neonatal EEG Findings' J.Clin. Neurophysiol, 28(2011): pp.185-189http://dx.doi. org/10.1097/WNP.0b013e3182121731 | Medline
- ASM Muthanantha Murugavel, S Ramakrishnan."Tree Based Wavelet Transform and DAG SVM for Seizure Detection.Signal and Image Processing": An International Journal, 3: pp. 115-125 (2012).
- N.V. Thakor *et al.* "Multi resolution Wavelet Analysis of Evoked Potentials", *IEEE Transactions on Biomedical Engineering*, 40(11): 1085-1093 (1993).
- S. Ventakaramanan, P. Prabhat, S.R Choudhury, H.B Nemade, and J.S. Sahambi. (2000).
 "Biomedical Instrumentation Based On Electrooculogram (EOG) Signal Processing And Application To A Hospital Alarm System", Indian Institute Of Technology (IIT) Gauhati, Proceedings of IEEE ICISEP, pp.535-539.
- Schlogl A, Keinrath C, Zimmermann D et al. A fully automated correction method of EOG artifacts in EEG recordings. *Clinical Neurophysiology*. 118: 98–104 (2007).
- Jung T-P, Makeig S, Humphries C, Lee T-W, McKeown MJ,Iragui V and Sejnowski TJ. Removing Electroencephalographic artifacts by blind source separation. *Psychophysiology.* 37: 163 –178 (2000a).
- Gratton G, Coles MG and Donchin E. A new method for off-line removal of oucular artifact. Electroencephalography Clin. *Neurophysiol.* 55: 484–486 (1983).
- M.Aminghafari, N. cheze, J.M Poggi, "Multivariate denoising using wavelets and principal component Analysis," *Computational* statistics & Data Analysis, 50: pp. 2381-2398 (2006).
- Pearson, K, "On Lines and Planes of Closest Fit to Systems of Points in Space", *Phil. Magazine*, 6(2): pp.559–572 (1901).
- 14. Hotelling. H," Analysis of a Complex of

Statistical Variables Into Principal Components", *J. Educ. Psychol.*, **24**: pp.417–441, pp.498–520 (1933).

- B. K. Kumar and K. V. S. V. R. Prasad, "Performance comparison of IST and multi scale principal component analysis in the EEG signal processing," 2017 International Conference on Computing Methodologies and Communication (ICCMC), Erode, 2017, pp. 536-542, doi: 10.1109/ICCMC.2017.8282523.
- 16. www.physionet.org
- 17. *www.mathworks.com/products/matlab/*, Discrete Wavelet Transform-2010.
- B.KrishnaKumar ,Dr.K.V.S.V.R.Prasad, Dr.K.Kishan Rao and Narsimha Baddiri, "Analysis of EEG Signals Using Multi-Scale Principal Component Analysis", IEEE Conference, Cape Institute of Technology, Levingapuram, Kanyakumari, pp.359-363: (2011).
- W.M.Bukhari W, Daud and Rubita Sudirman, "Time Frequency Analysis of Electrooculography (EOG) Signal of Eye Movement Potentials Based on Wavelet Energy Distribution",2011 Fifth Asia Modeling Symposium, pp.81-86 (2011).